

1 **HEART RATE REDUCTION IMPROVES BIVENTRICULAR FUNCTION AND**  
2 **INTERACTIONS IN EXPERIMENTAL PULMONARY HYPERTENSION**

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26

27 **ABSTRACT**

28 **Objectives:** To investigate mechanisms of heart rate (HR) reduction on biventricular function  
29 and interactions in experimental pulmonary arterial hypertension (PAH).

30 **Methods:** We compared cardiac-cycle mechanics and interventricular interactions in 15 sham, 8  
31 monocrotaline-PAH, 9 PAH+carvedilol and 8 PAH+ivabradine rats. We used echocardiography  
32 to assess biventricular function, timing of cardiac- cycle events and septal position in PAH rats;  
33 and related HR reduction effect on biventricular function measured by echocardiography and  
34 conductance catheter.

35 **Results:** HR was 302 in PAH+carvedilol , 303 in PAH+ivabradine vs. 359 bpm in PAH  
36 ( $p<0.01$ , respectively). Shams showed temporal alignment between right (RV) and left  
37 ventricular (LV) events; while PAH-rats showed increased biventricular isovolumic contraction  
38 times (ICT), delayed RV peak-radial motion and impaired early relaxation. Temporal  
39 malalignment was associated with decreased tricuspid and mitral diastolic annular peak  
40 velocities ( $E'$ ) (3.7 vs. 6.4 and 3.4 vs. 5.3,  $p<0.001$  respectively), delayed and shortened  
41 biventricular filling and reduced early-diastolic LV- filling ( $E$ ) velocity (0.56 vs. 0.81,  $p<0.01$ ).  
42 LV eccentricity index was increased in systole (2.0 vs. 1.2,  $p<0.001$ ), early-diastole (2.1 vs. 1.1,  
43  $p < 0.001$ ) and end-diastole (1.6 vs. 1.1,  $p<0.001$ ) in PAH vs. shams. HR reduction with  
44 carvedilol and ivabradine shortened biventricular ICT, time-to biventricular peak-radial motion,  
45 improved RV relaxation and increased early-diastolic LV filling through reduced inter-  
46 ventricular interaction and improved timing. These improvements corresponded with enhanced  
47 hemodynamics (increased cardiac-output, RV contractility and diastolic relaxation).

48 **Conclusions:** HR reduction by carvedilol and ivabradine improve biventricular filling and  
49 hemodynamics in experimental PAH through re-alignment of RV-LV cardiac-cycle events and  
50 improved interventricular interactions.

51 **KEY WORDS**

52 Pulmonary hypertension, ivabradine, carvedilol, heart rate reduction, interventricular  
53 interactions.

54 **NEW AND NOTEWORTHY**

55 Carvedilol improves biventricular function in experimental-PAH but the mechanisms of HR  
56 reduction vs. beta-blocker effect are inadequately defined. We demonstrate that reducing HR  
57 using either carvedilol or ivabradine ( $I_f$  inhibitor without beta-blocker effect), improves RV  
58 filling and biventricular hemodynamics through the re-alignment of RV-LV cardiac-cycle events  
59 and improved interventricular interactions.

60

61 **INTRODUCTION**

62 Right (RV) as well as left (LV) ventricular dysfunction drive mortality in pulmonary  
63 hypertension (PAH) (9, 15, 8) . We previously showed that the ratio of RV systolic to diastolic  
64 duration (S:D ratio) is increased in PAH children in association with worse exercise tolerance  
65 and survival (1). A high S:D ratio in PAH reflects prolonged leftward septal shift by the  
66 hypertensive RV and associated reduced LV filling, already compromised by the short diastolic  
67 duration; thereby reflecting adverse interventricular interactions (7) . With increasing heart rate  
68 (HR), diastole shortens and the S:D ratio increases exponentially; markedly so in PAH patients  
69 versus a much smaller change in controls (1,21) . Based on these clinical observations and on  
70 prior findings that carvedilol improves RV function in experimental PAH (2, 3) we hypothesized  
71 that reducing HR in PAH would prolong diastole and decrease the S:D ratio, and might improve  
72 interventricular interactions leading to increased filling. This formed the rationale for studying  
73 carvedilol's effects in experimental PAH (15). In that study, we found that carvedilol improved  
74 biventricular contractility and relaxation, measured by pressure-volume loops, reduced  
75 biventricular fibrosis, increased cardiac output, exercise capacity and a trend towards improved  
76 survival (15).

77 However, the impact of HR reduction on biventricular function, interventricular interactions and  
78 timing of events in the cardiac cycle in PAH is incompletely defined; and whether carvedilol  
79 improves biventricular function in experimental PAH through HR reduction or through  
80 adrenergic receptor blockade remains unknown.

81 Ivabradine is a selective inhibitor of the sinoatrial inward hyperpolarization-activated current ( $I_f$ )  
82 that reduces HR, without beta-blocker effects and without direct effects on global LV systolic  
83 function, coronary flow or pulmonary vascular resistance (22-24). Therefore, ivabradine

84 constitutes a very good tool to assess the effects of HR reduction on biventricular function in  
85 PAH, and to differentiate whether carvedilol's beneficial effects are due to HR reduction or due  
86 to its anti-adrenergic properties. Delineating these effects is important as morbidity and  
87 mortality in PAH remain high, therapeutic options limited and beta-adrenergic receptor blockers  
88 are relatively contraindicated in this condition (6, 19). We hypothesized that reducing HR  
89 improves interventricular interactions in PAH independent of beta-adrenergic blockade.  
90 Accordingly, we aimed to investigate the effects of carvedilol and ivabradine on cardiac-  
91 intervals and interventricular interactions in a rat model of PAH.

## 92 **GLOSSARY**

93 RV= right ventricle

94 PAH= pulmonary arterial hypertension

95 LV= left ventricle

96 S:D ratio= systolic to diastolic ratio

97 HR= heart rate

98 ECG=electrocardiogram

99 ICT= isovolumic contraction time

100 ET= ejection time

101 IRT= isovolumic relaxation time

102 TAPSE= tricuspid annular systolic excursion

103 MAPSE= mitral annular systolic excursion

104 IVS= interventricular septum

105 EC= eccentricity index

106 ICC= intraclass correlation coefficient for absolute agreement

107 SERCA2a=sarco-endoplasmic-reticulum- $\text{Ca}^{2+}$ -ATPase2a

108

109 **METHODS:**

110 We analyzed echocardiograms from male Sprague-Dawley monocrotaline-induced PAH rats  
111 (Charles River Laboratories, Senneville, Canada) from overlapping groups from previously  
112 reported experiment (15). For the purposes of this investigation we excluded 2 PAH rats from  
113 the original experiment that had profound terminal bradycardia at echocardiography and studied  
114 3 new animals not included in that experiment. For the current study we additionally studied a  
115 group of PAH rats treated with ivabradine. Animal care and experiments were conducted  
116 according to institutional Animal Ethic Committee and National Institutes of Health guidelines.

117 **Experimental Protocol:**

118 The experimental protocol has been described previously (15). Rats were 6-weeks old at protocol  
119 onset and randomly assigned to the following groups: (a) Shams: received a single subcutaneous  
120 injection of 0.9% saline (1 ml) (b) PAH: received a single subcutaneous injection of  
121 monocrotaline (60 mg/kg) to induce PAH, (c) PAH+carvedilol: rats were orally treated with  
122 carvedilol (15 mg/kg/day, for 3-weeks) and (d) PAH+ivabradine: rats were orally treated with  
123 ivabradine (10mg/kg/d, for 3-weeks), the last two groups starting therapy 2-weeks after  
124 monocrotaline injection. Rats were euthanized by cardiac extraction under deep isoflurane 3%  
125 anesthesia at the terminal experiment, 5-weeks after the start of the protocol.

126 **Echocardiography:**

127 Using a Vivid-E9 with 12-MHz phased-array transducer (General Electric, Wauwatosa, WI)  
128 under light isoflurane 3% sedation, 2D, M-mode, color and pulsed-Doppler were obtained with  
129 simultaneous electrocardiogram (ECG) display from rats surviving to the terminal experiment  
130 (5-weeks after the monocrotaline injection). Digital data were analyzed offline (EchoPac, version

131 8.0, GE). 3-cardiac cycles were analyzed using the ECG R-wave as a reference. Cardiac-cycle  
132 duration (RR-interval) and HR were recorded.

133 Tissue Doppler Imaging and Pulsed Doppler measurements:

134 Tricuspid and mitral inflows were recorded from an apical 4-chamber view. Tricuspid and  
135 mitral inflow early (E) and late (A) velocities were measured from 3 cardiac-cycles and the mean  
136 value calculated. As illustrated in **Figures 1A-B**, time to tricuspid valve and mitral valve  
137 opening were measured from the onset of the ECG R-wave to the onset of tricuspid and mitral  
138 Doppler flow, respectively. Right ventricular (RV) and left ventricular (LV) inflow duration  
139 were measured from the Doppler early diastolic (E)-wave onset to late diastolic (A)-wave  
140 termination. Pulmonary artery outflow was measured from a short-axis view. Pulmonary and  
141 aortic outflow were measured from short-axis and apical 5-chamber views, respectively. We  
142 used the conventional definition of the RV and LV isovolumic contraction times (ICT), as  
143 incorporating the electro-mechanical delay and isovolumic contraction time as measured from  
144 the onset of the ECG Q-wave to onset of pulmonary or aortic Doppler flow, respectively  
145 (**Figures 1C-D**). Ejection time (ET) was measured from pulmonary and aortic Doppler flows.  
146 LV isovolumic relaxation time (IRT) was measured from termination of aortic flow to onset of  
147 the following mitral E-wave using a Doppler sample straddling the LV inflow and outflow  
148 (**Figure 1D**). RV IRT was calculated as the time from pulmonary valve closure to tricuspid valve  
149 opening (ensuring images had the same HR, **Figure 1C**). For all timing measurements, 3-cardiac  
150 cycles were analyzed. We also recorded total cardiac-cycle duration (measured as the ECG, RR-  
151 interval) and HR. Tricuspid and mitral lateral annulus pulsed tissue Doppler velocities (systolic  
152 velocity ( $S'$ ), early ( $E'$ ) and late ( $A'$ ) diastolic velocities) were obtained from 3-cardiac cycles  
153 and the results averaged.



154 M-mode measurements:

155 Time to maximum tricuspid and mitral annular systolic excursion (TAPSE, MAPSE) were  
156 measured in an apical 4-chamber view from the ECG-R wave onset (**Figure 2**). Time to peak RV  
157 and LV free-wall radial thickening were measured from the short-axis (**Figure 3A**). The pattern  
158 and sequence of interventricular septal (IVS) motion and time to maximal early-diastolic LV  
159 septal bowing were evaluated by M-mode.

160 2D assessment and interventricular interactions:

161 The fractional area change (FAC) was calculated as end-diastolic-end-systolic/ end-diastolic RV  
162 areas from a 4-chamber view. The LV eccentricity index (EC) was obtained from a short-axis  
163 view at the LV papillary muscle level at end-systole, early-diastole and end-diastole (**Figure 4**).  
164 Images were analyzed frame-by-frame, simultaneously with the ECG, to describe the IVS  
165 configuration and position through the cardiac-cycle.

166 **Invasively measured hemodynamics:**

167 At the terminal experiment, hemodynamics were measured immediately after echocardiography  
168 using a high-fidelity 2F conductance catheter (Millar Instruments, Houston, Tx) under 3%  
169 isoflurane anesthesia. Cardiac output (CO), end-systolic and diastolic volumes and pressures  
170 were determined from pressure-volume loops. The maximal rate of ventricular pressure rise and  
171 decay ( $dp/dt$  max,  $dp/dt$  min) were calculated. Tau was assessed as the time constant of mono-  
172 exponential decay of ventricular pressure during isovolumic relaxation. Myocardial contractility  
173 (elastance,  $E_{es}$ ) was determined from a family of pressure-volume loops recorded during  
174 transient occlusion of the inferior vena cava. After measuring RV hemodynamics, the catheter  
175 was inserted through the LV apex to measure LV hemodynamics.

176 **Statistical analysis:**

177 All timing measurements were normalized to the RR-interval and expressed as percentage of the  
178 cardiac-cycle. Data are presented as mean  $\pm$  standard deviation. Differences between groups were  
179 analyzed with one-way analysis of variance and *post-hoc* least significant difference test (SPSS,  
180 IBM). Intra- and inter-observer reliability were evaluated in 20-rats (n=5/ group). A two-way  
181 mixed-model (targets conceived as random samples) intraclass correlation coefficient (ICC) for  
182 absolute agreement was calculated (5). A *p*-value  $< 0.05$  was considered significant.

### 183 **RESULTS:**

184 Forty rats were studied (15 shams, 8 PAH, 9 PAH+carvedilol, 8 PAH+ivabradine). Their body  
185 weight (significantly reduced in all PAH groups as compared to Sham) and echocardiographic  
186 timing measurements are summarized in **Table 1** and **Figures 3A-D**. Invasive hemodynamic and  
187 functional parameters were obtained from 8 shams, 5 PAH, 9 PAH +carvedilol rats and 7  
188 PAH+ivabradine rats (**Table 2**).

#### 189 Heart Rate

190 HR was reduced by 16% in the PAH+carvedilol and PAH+ivabradine groups vs. shams ( $302 \pm 22$   
191 and  $304 \pm 17$  beats per minute vs.  $359 \pm 31$  beats per minute,  $p < 0.001$  respectively). PAH rats had  
192 statistically similar HR as compared to shams ( $334 \pm 28$  vs  $359 \pm 31$  beats per minute,  $p = 0.295$ )  
193 (**Table 1**). The results of the LV+S/RV (Fulton) ratio were: control:  $0.28 \pm 0.03$ ; PAH:  $0.68 \pm 0.1$ ;  
194 PAH+carvedilol:  $0.55 \pm 0.12$ ; PAH+ivabradine:  $0.76 \pm 0.1$  (all  $p < 0.001$  vs. control).

#### 195 Cardiac-cycle events

196 In shams, the pulmonary and aortic valves open and close near-simultaneously (**Figure 3A**),  
197 while the tricuspid valve opens slightly after the mitral valve. Compared with shams, PAH-rats  
198 had significantly increased RV ICT, delayed tricuspid valve opening and reduced RV ET as well

199 as filling time. PAH-rats also showed increased LV ICT and reduced LV ET as well as filling  
200 time (**Figure 3B**). With HR reduction, RV ET and filling time remained short in PAH+carvedilol  
201 and PAH+ivabradine (**Figures 3C-D**) (due to high pulmonary vascular resistance, **Table 1**), but  
202 timings changed: RV as well as LV ICT shortened significantly, thus shifting timing of valve  
203 opening towards normality. Filling time (although only significantly for the LV with carvedilol)  
204 had a tendency to normalize.

205 The delay in RV cardiac-cycle events detailed above in PAH-rats correlated with a significant  
206 left-to-right radial motion misalignment between the RV and LV seen on M-mode. RV peak-  
207 radial motion occurred significantly later and for a longer duration (**Figure 3B**). Consequently,  
208 LV relaxation started while the RV was still contracting. RV and LV longitudinal shortening was  
209 largely simultaneous, but significantly delayed in PAH-rats (**Table 1, Figure 3B**) as compared to  
210 shams, in which RV and LV peak-radial motion and early-relaxation occurred simultaneously,  
211 coinciding with peak-longitudinal TAPSE and MAPSE (**Figure 3A**). Due to prolonged RV  
212 systole, reduced RV ejection time in PAH-rats, RV filling time was significantly shortened  
213 (**Table 1**) and delayed to late-diastole, coinciding with atrial contraction (**Figure 3B**). As shown  
214 in **Table 1**, these findings were also associated with reduced tricuspid and mitral lateral annulus  
215 tissue Doppler systolic ( $S'$ ), early ( $E'$ ) and late ( $A'$ ) diastolic velocities. The addition of  
216 carvedilol and ivabradine significantly improved LV-RV radial contractile alignment (**Figures**  
217 **3C-D**), with RV free-wall peak-radial contraction occurring earlier; and as observed on M-mode,  
218 faster early RV relaxation (**Figures 3B-D**). Carvedilol also reduced times to peak TAPSE and  
219 MAPSE compared with the PAH-group (**Table 1, Figure 3C**) and normalized both tricuspid and  
220 mitral lateral annulus systolic and diastolic velocities (**Table 1**). Ivabradine reduced time to peak

221 TAPSE compared with PAH-group (**Table 1, Figure 3D**) but its effects on tricuspid and mitral  
222 annulus systolic and diastolic velocities were more modest (**Table 1**).

### 223 Interventricular interactions

224 Visual analysis of M-mode in shams showed simultaneous IVS, RV and LV lateral free-wall  
225 motion, without early-diastolic LV septal bowing (**Figure 3A**). Conversely, 90% of PAH-rats  
226 showed early-diastolic leftward septal bowing as a consequence of LV-RV disparate radial  
227 motion and delayed RV relaxation described above (**Figure 3B**). Frame-by-frame 2D assessment  
228 of IVS configuration in the short-axis view confirmed M-mode findings: shams had a circular  
229 LV with normal round IVS curvature and position throughout the cardiac-cycle (**Figure 4A**),  
230 while in PAH-rats the RV was markedly enlarged, the LV flattened and ‘D-shaped’ throughout  
231 the cardiac-cycle (**Figure 4B**); with the IVS displaced leftward in systole and early-diastole and  
232 flattened into late-diastole. These findings were associated with significantly higher LV EC  
233 throughout the cardiac-cycle in PAH-rats vs. controls (**Table 1**). Based on visual M-mode  
234 assessment (**Figures 3C-D**) carvedilol and ivabradine led to faster early RV relaxation and  
235 significantly reduced time to maximal LV septal bowing compared with untreated PAH-rats  
236 (**Table 1, Figures 3B+D**). This corresponded with the shorter tau found in these animals (**Table**  
237 **2**). Moreover, carvedilol significantly reduced LV EC index in systole and early-diastole (**Table**  
238 **1**). Although the RV remained enlarged and TV inflow duration short in both treated groups, the  
239 improvement in interventricular coupling in early-diastole translated into an increased early  
240 diastolic LV filling (E) velocities and normalized lateral mitral annular peak diastolic tissue  
241 velocities (**Table 1**). Biventricular early-systolic function was also improved with carvedilol as  
242 reflected by reduced time to maximal TAPSE and MAPSE and increased tricuspid and mitral  
243 lateral annular peak-systolic tissue velocities (**Table 1**).

244 Hemodynamics and function:

245 Hemodynamics and function variables are summarized in **Table 2**. RV peak systolic pressure  
246 and RV/LV systolic pressure ratio were increased in all PAH groups vs. shams and not different  
247 between PAH groups. The improved RV and LV mechanics, timing and interventricular  
248 interactions detailed above with HR reduction corresponded with improved hemodynamics as  
249 seen by increased CO, RV contractility (dP/dTmax, Ees) and diastolic relaxation (dP/dTmin,  
250 Tau).

251 Intra-observer and inter-observer reliability:

252 Intra-observer and inter-observer reproducibility for echo measurements was good (**Table 3**).

253 **DISCUSSION:**

254 We evaluated the mechanical effects of HR reduction on cardiac-cycle events and function in  
255 experimental PAH. We demonstrate that despite persistent PAH, carvedilol and ivabradine  
256 improve early RV relaxation and realign RV-LV radial motion by reducing biventricular ICT  
257 and normalizing longitudinal biventricular motion. In particular, these effects improve early LV  
258 filling and therefore biventricular systolic and diastolic function and hemodynamics. This  
259 detailed analysis provides a mechanistic basis for carvedilol's beneficial effects on biventricular  
260 function in PAH and strengthens the basis for investigating its use in clinical PAH (15, 2,3).

261 Heart-rate effects

262 Improved interventricular interactions were at least partially, attributable to HR. However,  
263 although carvedilol and ivabradine significantly decreased HR in PAH-rats, RV diastolic  
264 duration did not lengthen significantly nor did ejection time shorten. Nonetheless, we observed  
265 improvements in biventricular diastolic function and ventricular filling. Of note, the mean HR  
266 was not different in the PAH-group compared to shams, which differs from the PAH-rats

267 presented in our previous experiment (15). This difference may be explained by 3 rats not being  
268 the same individuals.

### 269 Systolic radial alignment

270 Carvedilol led to re-alignment of RV-LV peak-radial motion. Earlier RV peak-radial motion in  
271 the PAH+HR reduction was associated with significant biventricular ICT shortening (**Table 1**).  
272 Left-right delay in peak myocardial shortening in PAH patients is caused by prolonged rather  
273 than delayed RV contraction (12) including increased ICT. This causes early-diastolic LV septal  
274 bowing, decreased LV filling and decreased stroke volume, all important features in the PAH-  
275 group. Computer modeling suggests that electrically pre-exciting the RV leads to simultaneous  
276 RV-LV contraction thereby improving biventricular function and filling (11). We now show  
277 similar beneficial effects on these critical events with carvedilol and ivabradine, despite  
278 persistent PAH. Moreover, we demonstrate inefficient RV contraction in PAH as RV peak-radial  
279 contraction occurs after pulmonary valve closure, and close to tricuspid valve opening (**Figure**  
280 **3B**), consistent with RV post-systolic contraction present in PAH patients (12, 13). Overall, HR  
281 reduction improved interventricular radial mechanical synchrony due to earlier and shorter ICT  
282 and better aligned RV radial mechanics.

### 283 Improvements in systolic and diastolic function

284 RV contractility and relaxation were improved with HR reduction using pressure-volume loop  
285 derived end-systolic elastance, time-constant of RV relaxation ( $\tau$ ) and  $dP/dT$  minimum (**Table**  
286 **2**). These are consistent with the improved RV relaxation seen by M-mode and tissue Doppler  
287 velocities in the current study, and associated with improved LV filling. Early RV relaxation, as  
288 measured by  $\tau$  and decreased diastolic tissue Doppler velocities, is abnormal in clinical PAH  
289 even when contractility is still preserved early in the disease course (14, 4). Both impaired

290 relaxation and post-systolic contraction compromise diastolic function (12, 13). In the present  
291 study we demonstrate that carvedilol and ivabradine not only improve RV relaxation and  
292 diastolic performance as seen by tissue Doppler imaging, M-mode and Doppler flow, but also  
293 enhance biventricular function in early systole. Thus, improved RV relaxation seems important  
294 in explaining not only improved RV diastolic, but also systolic function, S:D ratio and early-  
295 diastolic interventricular interactions. Together, the re-alignment of radial mechanics and earlier  
296 longitudinal motion towards normal induced by HR reduction, lead to improved early-diastolic  
297 LV geometry and improved LV filling in early diastole. Peak systolic pressure and cardiac  
298 output in the PAH-ivabradine group tended to be higher than the PAH-carvedilol group. The  
299 carvedilol treated group may have somewhat lower peak systolic pressures and cardiac output  
300 due to a negative inotropic effect versus ivabradine. However, the RV/LV pressure ratio was the  
301 same in all groups allowing comparison between them in terms of the PAH.

### 302 Postulated mechanisms of action

303 We did not study the molecular mechanisms underlying the biventricular mechanics investigated  
304 in the current study, but these are worthy of a short hypothesis-generating discussion. As  
305 ivabradine induced similar effects to carvedilol, the effects could be attributable to a lower HR.  
306 However, rather than lengthening RV and LV filling time per se, the effect is based on a change  
307 in the timing of events, where ICT shortens and leads to a normalization of the timings in the  
308 cardiac cycle that were importantly changed due to the PAH. Related to this, the interventricular  
309 interaction changes with HR reduction, thereby attenuating the important septal shift in early  
310 diastole. From M-mode images, a restoration of the early outwards motion of the RV wall can be  
311 seen, thus also improving early LV filling. While it is difficult to completely distinguish between  
312 HR reducing effects versus other components of beta-blocker effects of carvedilol, the similar

313 improvement in ventricular function and contractility seen in both the carvedilol and ivabradine  
314 treated groups suggests that it is HR reduction, rather than beta-blockade per se, that leads to  
315 improved function. We postulate that this occurs through re-alignment of RV and LV events and  
316 improved diastolic relaxation.

317 The exact mechanisms remain to be elucidated. One postulated mechanism may relate to the  
318 timing of actin-myosin cross-bridging. Increased afterload reduces myocyte shortening velocity  
319 and prolongs shortening (25). Thus, RV pressure remains higher for a longer duration than the  
320 LV. Consequently, RV actin-myosin cross-bridge cycling may lengthen (hyper-bridging)  
321 resulting in stiffer myocardium at end-ejection, prolonging IRT and hampering early-relaxation.  
322 Although not proven in this study, HR reduction and associated changes in ICT may improve RV  
323 early-relaxation by reducing actin-myosin crossbridging, resulting in more compliant  
324 myocardium at end-systole (25, 10). This could explain the observed improvements in RV  
325 relaxation, contractility, LV-RV interactions and LV early-diastolic filling, as well as the trend to  
326 reduced RV and LV end-diastolic pressures.

327 We previously showed that carvedilol upregulates RV sarco-endoplasmic-reticulum- $\text{Ca}^{2+}$ -  
328 ATPase2a (SERCA2a) expression in experimental PAH with a similar trend in the LV (15).  
329 Downregulated SERCA2a in failing myocardium impairs intracellular calcium cycling, affecting  
330 troponin-C binding and actin-myosin crossbridging, worsening contractile and diastolic function  
331 (17). Conversely, restoration of SERCA2a improves calcium cycling and cardiac function (17).  
332 Based on our current results and prior findings, we hypothesize that HR reduction may improve  
333 calcium handling and myocardial relaxation by restoring SERCA2a. This requires confirmation  
334 in further studies. Likewise, we previously found biventricular fibrosis in PAH-rats and its  
335 amelioration with carvedilol through downregulated transforming-growth-factor-beta signaling



336 (15). Decreased fibrosis may further explain the observed improvement in systolic and diastolic  
337 performance, reduced leftward septal bowing and improved interventricular interactions.  
338 Likewise, in our prior study, RV and LV cardiomyocyte diameter were increased with PAH and  
339 decreased with carvedilol (reaching statistical significance for the RV), albeit not to baseline size  
340 (15). Whether there is a differential effect of pure HR reduction (ivabradine) or additional  
341 contractility modulation (carvedilol) remains to be studied.

#### 342 Possible Clinical implications

343 Many PAH patients expire from RV failure (9), but cardiac-specific treatments are lacking (6).  
344 Beta-adrenergic receptor blockers, and HR reduction in general, improve heart function and  
345 survival in left heart failure (16), but are currently contraindicated in PAH because of potential  
346 detrimental effects on cardiac output (19). However, we and others have demonstrated in  
347 experimental PAH, that beta-adrenergic receptor blockers, and selective inhibition of the  
348 sinoatrial inward hyperpolarization-activated current, improve biventricular function, stroke  
349 volume, cardiac output and exercise capacity, despite persistent PAH (15, 3, 18). These changes  
350 were accompanied by a lower RV S:D ratio (15), a clinically relevant finding as increased S:D  
351 ratio is associated with mortality in pediatric PAH (1). Moreover, in early PAH, the RV  
352 maintains contractility, but there may be coexisting abnormal early relaxation (14). The results of  
353 the current study suggest the need for carefully controlled human trials to test the safety and  
354 efficacy of HR reduction in PAH recognizing that the density and distribution of cardiac  
355 adrenergic receptors (in the case of beta-blockers) can differ between rodents and humans, which  
356 can impact the clinical implications of our findings.

#### 357 Study limitations

358 The aim of the present study was to investigate carvedilol's and ivabradine's effects on cardiac-  
359 cycle events and mechanics in PAH and we did not evaluate molecular mechanisms. Likewise,  
360 we did not directly assess RV compliance or crossbridging. The limitations of experimental PAH  
361 models are well known. Relevant to the current study, we previously demonstrated in a  
362 monocrotaline-PAH that carvedilol did not act through alleviation of myocarditis or lung  
363 inflammation, both absent in these animals (15). Importantly, PAH was persistent, allowing  
364 study of carvedilol's and ivabradine's biventricular effects without the confounding effect of  
365 decreased pulmonary vascular resistance. The 12-mHz probe used in this study is of relatively  
366 low frequency. However, we have found that in rats the 12-Mhz transducer often produces better  
367 quality images than very high frequency transducers designed predominantly for use in mice and  
368 have recently reported good feasibility and reproducibility using a 10 Mhz probe in a rabbit  
369 model (20). In the current study, we also performed inter and intra-observer reliability which was  
370 found to be good (Table 3). Moreover, the same probe was used across all groups and thus the  
371 comparison is subject to the same conditions and is valid.

### 372 Conclusion

373 In conclusion, we demonstrate that in experimental PAH, HR reduction improves RV early-  
374 relaxation and diastolic function, leading to re-alignment of systolic RV-LV peak-radial  
375 mechanics and interventricular interactions. These improved mechanics and biventricular  
376 function were associated with improved cardiac output and hemodynamics.

### 377 **Disclosures**

378 None

379

380

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	Sham (n=15)	PAH (n=8)	PAH +carvedilol (n=9)	PAH+ ivabradine (n=8)
Body weight (gr)	472.6±48.6	397.1±53.3*	403.6±73.8*	349.2±22.1**
HR (bpm)	359± 31.2 <sup>§§§,μμμ</sup>	334± 27.6	302.5 ± 21.8 <sup>***</sup>	303.6± 17.1 <sup>***</sup>
RR- interval (ms)	167.6 ± 14.9 <sup>§§§,μμμ</sup>	180.1± 15.2	198.5± 14.5 <sup>***</sup>	198.5± 12.2 <sup>***</sup>
<b>Functional parameters</b>				
TV E (cm/s)	0.50 ± 0.1	0.69 ± 0.1	0.57 ± 0.3	0.54 ± 0.1
TV A (cm/s)	0.70 ± 0.1	0.55 ± 0.1	0.69 ± 0.3	0.54 ± 0.2
RV E'(cm/s)	6.4 ± 2.1 <sup>tt,μ</sup>	3.7 ± 1.3 <sup>**,§</sup>	6.0 ± 1.2 <sup>†</sup>	4.25± 0.7*
RV A'(cm/s)	6.1 ± 1.8 <sup>†</sup>	4.0 ± 1.5*	5.0 ± 1.4	4.1 ± 1.5
RV S'(cm/s)	6.3 ± 1.3 <sup>ttt</sup>	3.5 ± 0.6 <sup>***,§§,μμ</sup>	6.1 ± 1.5 <sup>tt</sup>	5.9 ± 1.1 <sup>tt</sup>
RV FAC (%)	43.0± 5.0 <sup>ttt,§</sup>	24.5 ± 7.1 <sup>***,μμ</sup>	33.8 ± 7.6*	36.1 ± 7.3 <sup>tt</sup>
MV E (cm/s)	0.81 ± 0.1 <sup>tt</sup>	0.56 ± 0.1 <sup>**</sup>	0.71 ± 0.2	0.67± 0.1
MV A (cm/s)	0.74 ± 0.1	0.65 ± 0.1	0.64 ± 0.2	0.58± 0.1
LV E'(cm/s)	5.3 ± 1.1 <sup>tt</sup>	3.4 ± 1.1 <sup>**,§§,μ</sup>	5.3 ± 1.1 <sup>†</sup>	4.9± 0.1 <sup>†</sup>
LV A'(cm/s)	6.2 ± 0.4 <sup>t,μ</sup>	4.5 ± 2.0*	4.7 ± 1.8	4.4 ± 0.9*
LV S'(cm/s)	6.8 ± 1.3 <sup>†</sup>	4.6 ± 2.0*	5.9 ± 1.7	6.25± 1.5
<b>Left ventricle eccentricity index</b>				
End-systolic EC	1.2 ± 0.1 <sup>ttt,μμ</sup>	2.0 ± 0.4 <sup>***,§§</sup>	1.4 ± 0.3 <sup>tt</sup>	1.70 ± 0.3 <sup>**</sup>
Early-diastolic EC	1.1 ± 0.1 <sup>ttt,μμμ</sup>	2.1 ± 0.5 <sup>***,§§</sup>	1.5 ± 0.4 <sup>tt</sup>	1.9 ± 0.4 <sup>***</sup>
End-diastolic EC	1.1± 0.1 <sup>ttt,§,μμμ</sup>	1.6 ± 0.3 <sup>***</sup>	1.4 ± 0.3*	1.6 ± 0.3 <sup>***</sup>
<b>Pulsed Doppler timing parameters</b>				
RV ICT	15.2 ± 3.7 <sup>tt</sup>	21.8 ± 3.3 <sup>**,§,μ</sup>	15.6 ± 6.4 <sup>†</sup>	15.9 ± 1.7 <sup>†</sup>
RV ET	44.0 ± 4.0 <sup>tt,§§,μμ</sup>	35.7 ± 3.6 <sup>**</sup>	35.4 ± 9.2 <sup>**</sup>	35.9 ± 2.0 <sup>**</sup>
Time-to-PVC	59.2 ± 6.5 <sup>§</sup>	57.3 ± 3.6	48.4± 13.4*	51.75± 3.21
Time-to-TVO	70.3 ± 6.4	77.7 ± 8.9 <sup>§,μμ</sup>	66.5 ± 8.6 <sup>†</sup>	64.5± 4.0 <sup>tt</sup>
RV inflow duration	41.2 ± 5.5 <sup>ttt,§§,μ</sup>	26.8 ± 3.4 <sup>***</sup>	30.1 ± 7.2 <sup>**</sup>	32.1 ± 7.3 <sup>**</sup>
RV IRT	10.6 ± 4.5	23.1 ± 15.5	18.9 ± 17.5	14.1± 2.7
LV ICT	15.8± 4.2 <sup>ttt</sup>	23.6 ± 4.9 <sup>***,§§§,μ</sup>	14.0 ± 3.0 <sup>ttt</sup>	17.5 ± 2.6 <sup>tt</sup>
LV ET	42.1 ± 4.1 <sup>ttt,§§§,μμμ</sup>	30.7 ± 3.7 <sup>***</sup>	31.0 ± 3.4 <sup>***</sup>	31.0 ± 3.0 <sup>***</sup>
Time-to-AVC	57.9 ± 6.9 <sup>§§§,μμ</sup>	54.4 ± 4.3 <sup>§§</sup>	45.0 ± 4.2 <sup>***,tt</sup>	48.4± 1.9 <sup>**</sup>
Time-to-MVO	68.6 ± 6.2 <sup>§§</sup>	70.7 ± 3.9 <sup>§§,μ</sup>	60.5 ± 6.1 <sup>**,tt</sup>	63.0 ± 4.2 <sup>†</sup>
LV inflow duration	39.3 ± 2.9 <sup>†</sup>	33.3 ± 4.8 <sup>*,§</sup>	39.3 ± 5.6 <sup>†</sup>	37.7 ± 5.0
LV IRT	12.9 ± 2.4	15.5 ± 3.1	14.9 ± 2.4	13.8 ± 2.3
<b>M-mode timing parameters</b>				
Time-to-RV peak-radial motion	58.0 ± 5.1 <sup>ttt</sup>	71.3 ± 10.0 <sup>***,§§§,μμ</sup>	54.6 ± 6.8 <sup>ttt</sup>	58.6 ± 8.6 <sup>tt</sup>
Time- to- LV peak- radial motion	58.5 ± 5.8 <sup>§§§,μμ</sup>	54.9 ± 5.5	46.3 ± 11.2 <sup>**</sup>	48.6 ± 7.5 <sup>**</sup>
Time-to- maximum LVSB	----	75.5 ± 9.6 <sup>§,μ</sup>	59.7 ± 9.5 <sup>†</sup>	63.2 ± 9.2 <sup>†</sup>
Time-to-maximum TAPSE	57.3 ± 6.8 <sup>tt</sup>	69.2 ± 6.6 <sup>***,§§§,μμ</sup>	50.3 ± 8.8 <sup>ttt</sup>	57.0 ± 5.7 <sup>ttt</sup>

Time-to-maximum MAPSE                      56.0 ± 8.1<sup>†</sup>                      66.9 ± 3.6<sup>\*\*.§§</sup>                      51.3 ± 10.5<sup>‡‡</sup>                      56.3 ± 8.1

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**Table 1. Summary of echo measurements.** Data shown as mean ± SD. Timing measurements are normalized to their RR-interval and are expressed as percentages. PAH= pulmonary hypertension, HR= heart rate, bpm= beats per minute, ms= milliseconds. **Functional echocardiographic parameters:** TV=tricuspid valve, MV= mitral valve, LV= left ventricle, RV= right ventricle, FAC= Fractional area change. **Doppler timing:** ICT= isovolumic contraction time, ET=ejection time, PVC= pulmonary valve closure, TVO= tricuspid valve opening, AVC= aortic valve closure, MVO= mitral valve opening, IRT= isovolumic relaxation time. **M-mode timing:** IVS= interventricular septum, LVSB= early-diastolic LV septal bowing, TAPSE= tricuspid systolic annular excursion, MAPSE= mitral systolic annular excursion.

\*p<0.05, \*\*p<0.01, \*\*\*p<0.001 vs sham rats.  
†p<0.05, ‡p<0.01, ‡‡p<0.001 vs PAH rats.  
§p<0.05, §§p<0.01, §§§p<0.001 vs PAH-carvedilol rats.  
μp<0.05, μμp<0.01, μμμp<0.001 vs PAH-ivabradine rats.



	Sham (n=8)	PAH (n=5)	PAH +carvedilol (n=9)	PAH + ivabradine (n=7)
CO (mL/min)	103.6 ± 60.5	34.9 ± 22.3	57.9 ± 33.8	79.8 ± 27.4
<b>Right ventricle parameters</b>				
Peak Systolic pressure (mmHg)	23.4 ± 1.9 <sup>‡,§§,μμμ</sup>	58.1 ± 21.6 <sup>*</sup>	55.4 ± 24.5 <sup>**</sup>	68.1 ± 14.9 <sup>***</sup>
End-diastolic pressure (mmHg)	1.7 ± 1.2	3.7 ± 2.9	1.43 ± 1.3	2.5 ± 1.6
dP/dt max (mmHg/sec)	1011.7 ± 397.6 <sup>§§,μμμ</sup>	1739.7 ± 457	1980.2 ± 696.7 <sup>**</sup>	2313.8 ± 430.9 <sup>***</sup>
dP/dt min (mmHg/sec)	-740.0 ± 166.1 <sup>§,μ</sup>	-1720.5 ± 671	-1827.9 ± 1006.9 <sup>*</sup>	-2063.3 ± 840.8 <sup>*</sup>
Ees (mmHg/mL)	121.4 ± 90.2	26.9 ± 11.2	114.7 ± 69.8	191.4 ± 70.3
Tau (ms)	7.00 ± 1.4 <sup>††</sup>	13.2 ± 2.4 <sup>*,μ</sup>	10.11 ± 2.9	8.6 ± 2.2 <sup>†</sup>
<b>Left ventricle parameters</b>				
Peak Systolic pressure (mmHg)	78.1 ± 14.1	65.4 ± 17.9	66.1 ± 22.7	76.0 ± 26.7
End-diastolic pressure (mmHg)	3.9 ± 0.7	3.4 ± 3.0	2.5 ± 1.5	4.0 ± 1.2
dP/dt max (mmHg/sec)	3195.2 ± 618.2	2768.3 ± 1212	3048.9 ± 1389.0	3236.4 ± 1133.1
dP/dt min (mmHg/sec)	-2650.4 ± 649.6	-1537.2 ± 822	-1989.3 ± 1035.9	-1804.8 ± 706.0
Ees (mmHg/mL)	289.7 ± 344.0	53.8 ± 11.0	330.7 ± 284.6	157.3 ± 93.2
Tau (ms)	8.6 ± 1.5	9.3 ± 4.9	9.3 ± 3.9	8.0 ± 2.4
RVp/LVp	0.3 ± 0.1 <sup>†,§§,μμ</sup>	0.9 ± 0.3 <sup>*</sup>	0.9 ± 0.3 <sup>**</sup>	0.9 ± 0.2 <sup>**</sup>

470

471 **Table 2. Summary of invasive hemodynamic and functional parameters.** Data shown as mean ± SD. PAH=

472 pulmonary hypertension, CO= cardiac output, Ees= end-systolic elastance.

473 \*p<0.05, \*\*p<0.01, \*\*\*p<0.001 vs sham rats.

474 †p<0.05, †† p<0.01, ††† p<0.001 vs PAH rats.

475 § p<0.05, §§ p<0.01, §§§ p<0.001 vs PAH-carvedilol rats.

476 μ p<0.05, μμ p<0.01, μμμ p<0.001 vs PAH-ivabradine rats.

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Echocardiographic parameter	Intra-observer ICC	95%-CI	<i>p</i> *	Inter-observer ICC	95%-CI	<i>p</i> *
t-MVO	0.95	(0.81-0.98)	0.000	0.92	(0.57-0.98)	0.000
RV ICT	0.78	(0.24-0.94)	0.011	0.96	(0.88-0.99)	0.000
t-LV peak-radial motion	0.86	(0.54-0.96)	0.001	0.82	(0.44-0.94)	0.002
t-maximum TAPSE	0.76	(0.14-0.93)	0.016	0.92	(0.76-0.97)	0.000
LV End-systolic EC	0.78	(0.34-0.93)	0.003	0.63	(-0.03-0.87)	0.024

479

480 **Table 3. Intra-observer and inter-observer variability.** ICC= intraclass correlation coefficient; 95%-CI= 95%  
481 confidence interval; RV= right ventricle, LV= left ventricle, t-MVO=time-to-mitral valve opening; ICT= isovolumic  
482 contraction time; t-LV=time-to-LV peak-radial motion; t-TAPSE=time-to-maximum tricuspid systolic annular  
483 excursion; EC=eccentricity index. *p*\* < 0.05 considered significant.

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487 **FIGURES TITLES AND LEGENDS**

488

489 **Figure 1: Panel A:** Timing measurements of tricuspid valve inflow. Time to tricuspid valve  
490 opening (measurement **a**) was measured from the onset of the ECG R-wave to the onset of  
491 tricuspid flow. Right ventricle inflow duration (measurement **b**) was measured from the early  
492 diastolic (E)-wave onset to late diastolic (A)-wave termination. Time from closure-to opening of  
493 the tricuspid valve (measurement **c**) was calculated from late diastolic (A)-wave termination to  
494 the next early diastolic (E) wave onset. **Panel B:** Timing measurements of mitral valve inflow.  
495 Time to mitral valve opening (measurement **a**) was measured from the onset of the ECG R-wave  
496 to the onset of mitral flow. Left ventricle inflow duration (measurement **b**) was measured from  
497 the early diastolic (E)-wave onset to late diastolic (A)-wave termination. **Panel C:** Pulmonary  
498 outflow from a short axis right ventricle outflow view. Right ventricle isovolumic contraction  
499 time (measurement **d**) was measured from the onset of ECG R-wave to the onset of the  
500 pulmonary flow. Ejection time (measurement **e**) was measured from pulmonary flow (\*  
501 pulmonary valve closure). Right ventricular isovolumic relaxation time was calculated from  
502 closure-to opening of the tricuspid valve (measurement **c** from panel A; including the isovolumic  
503 contraction + the ejection + the isovolumic relaxation times) and then subtracting the isovolumic  
504 contraction (measurement **d**) +the ejection time (measurement **e**) from that interval. **Panel D:**  
505 Simultaneous sampling of aortic outflow and mitral inflow from an apical 5-chamber view. Left  
506 ventricle isovolumic contraction time (measurement **d**) was measured from the onset of ECG R-  
507 wave to the onset of the aortic flow. Ejection time (measurement **e**) was measured from aortic  
508 flow (\* aortic valve closure). Left ventricular isovolumic relaxation time (measurement **f**) was  
509 measured from termination of the aortic flow to the onset of mitral early diastolic flow (E-wave).  
510 The total cardiac cycle was defined as the ECG RR interval.

511

512

513 **Figure 2:**  $t$  = time from the onset of the ECG R-wave (dotted line) to the maximum tricuspid  
514 annular systolic excursion (TAPSE) and mitral annular systolic excursion (MAPSE) by M-mode,

515 in an apical 4-chamber from a rat with pulmonary arterial hypertension. The total cardiac cycle  
516 was defined as the ECG RR interval.

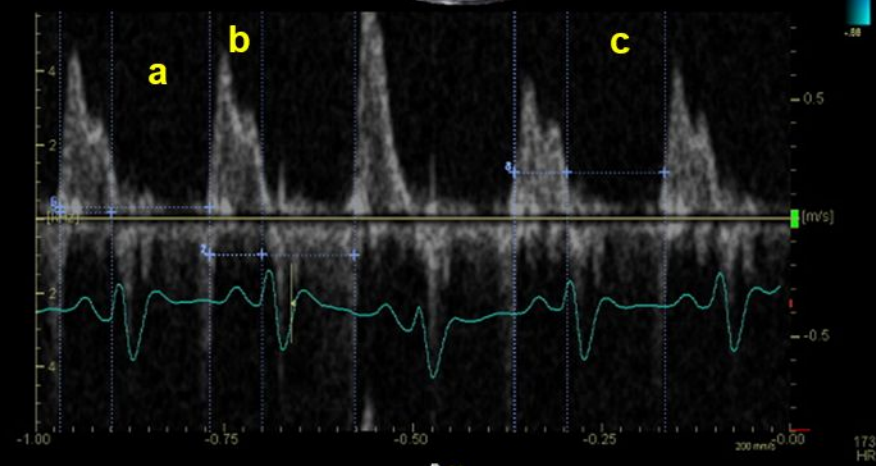
517  
518 **Figure 3:** Left: M-mode echocardiography depicting left (LV) and right ventricular (RV) free-  
519 wall radial motion in **panel A)** sham, **panel B)** PAH, **panel C)** PAH+carvedilol and **panel D)**  
520 PAH+ivabradine. PAH= pulmonary hypertension. (\*\*) Marks the bowing of the interventricular  
521 septum (IVS) towards the left in LV early-diastole (LVSB). Mean RR-interval by group is  
522 shown. Right: Schematic representation of the summary of timing measurements: **panel A)**  
523 sham, **panel B)** PAH, **panel C)** PAH+carvedilol and **panel D)** PAH+ivabradine. **Doppler**  
524 **timing:** PVO= pulmonary valve opening, AVO= aortic valve opening, PVC= pulmonary valve  
525 closure, AVC= aortic valve closure, TVO= tricuspid valve opening, MVO= mitral valve  
526 opening. **M-mode timing:** RV= RV peak-radial motion, LV= LV peak-radial motion, tTAPSE=  
527 maximum tricuspid systolic annular excursion, tMAPSE= maximum mitral systolic annular  
528 excursion.

529  
530 **Figure 4:** Short-axis view at left ventricular (LV) papillary muscles level in **panel A)** sham,  
531 **panel B)** PAH , **panel C)** PAH+carvedilol and **panel D)** PAH+ivabradine. PAH= pulmonary  
532 arterial hypertension. RV= right ventricle. The position of the interventricular septum (\*\*)  
533 throughout cardiac-cycle is shown.

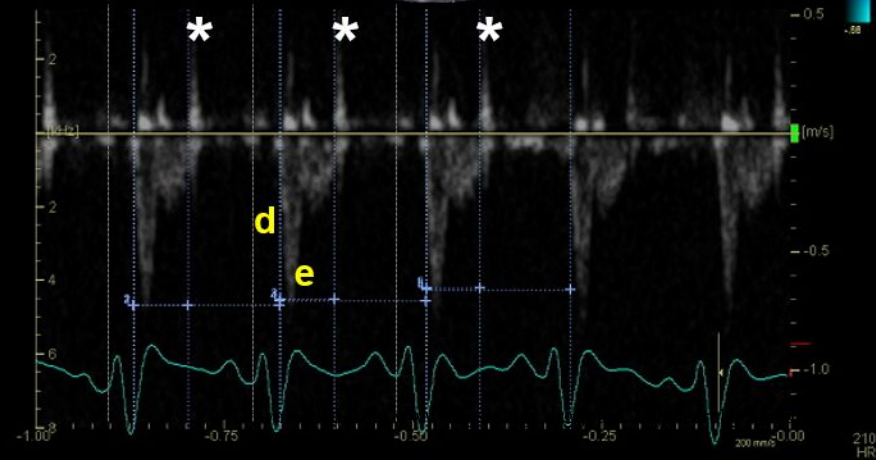
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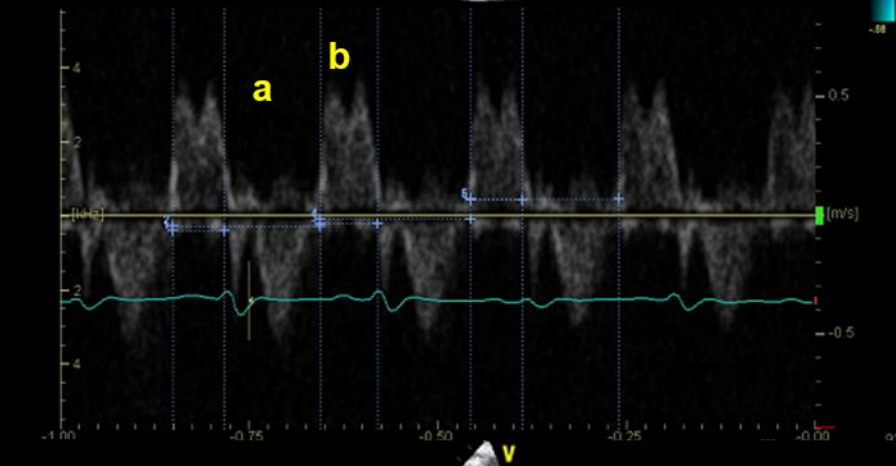
### A) Tricuspid flow



### C) Pulmonary flow



### C) Mitral flow



### D) Aortic flow

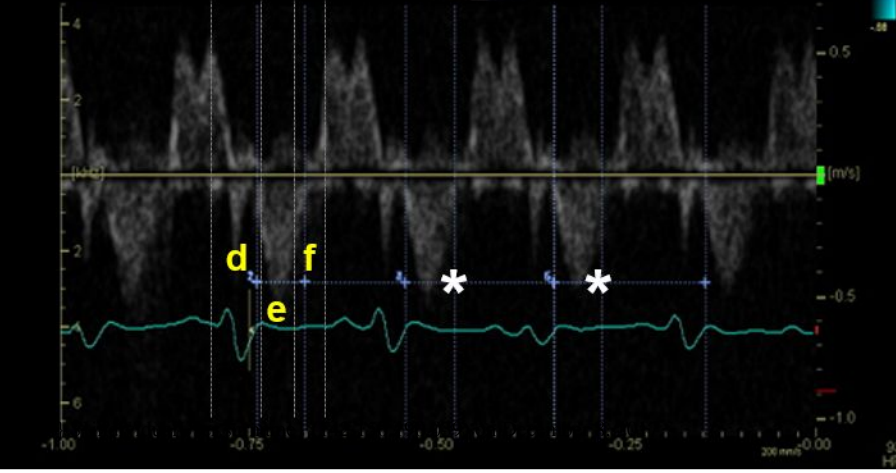
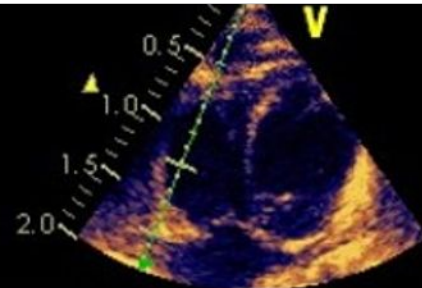


Figure 1

given

TAPSE



MAPSE

Figure 2

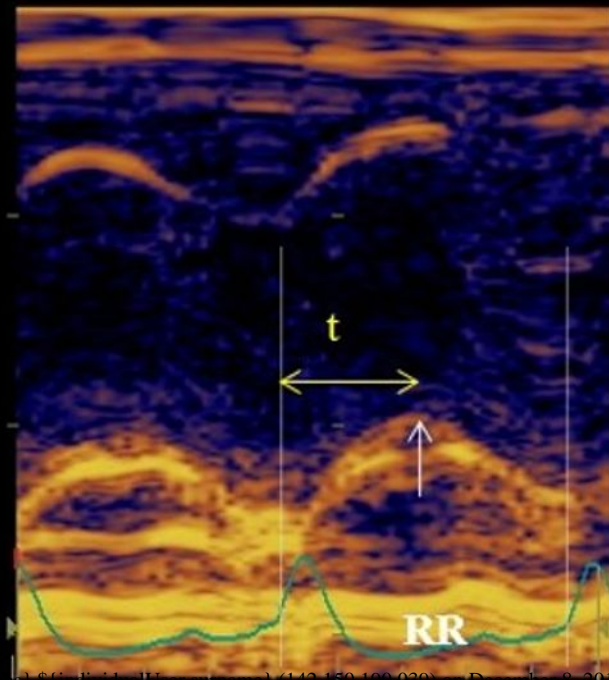
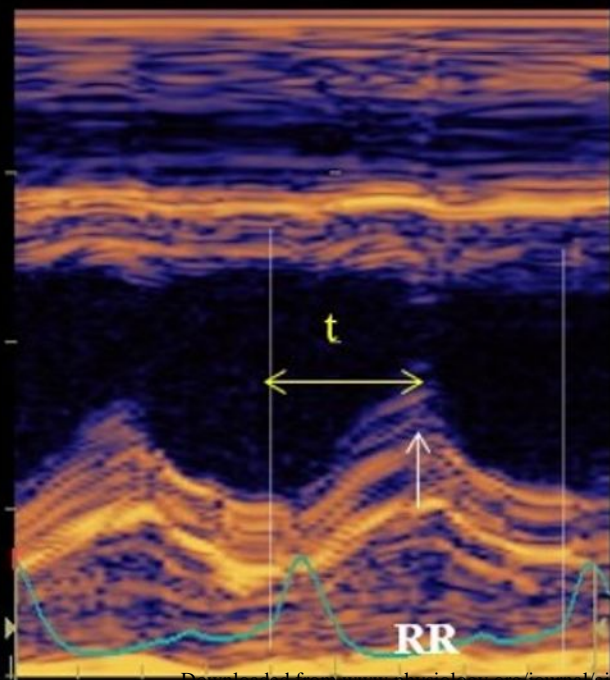
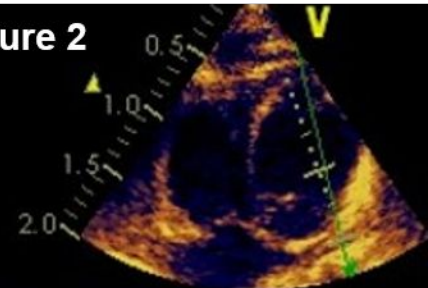
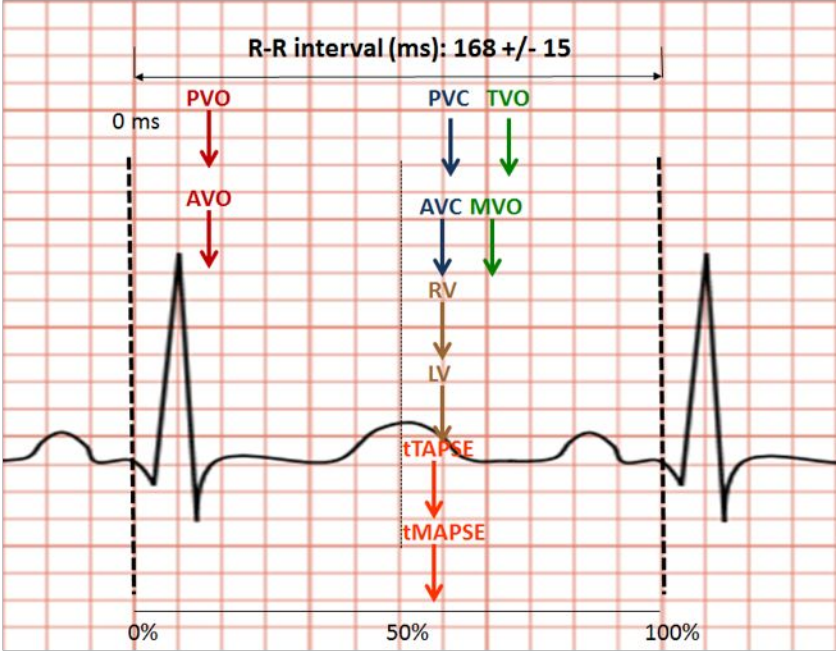
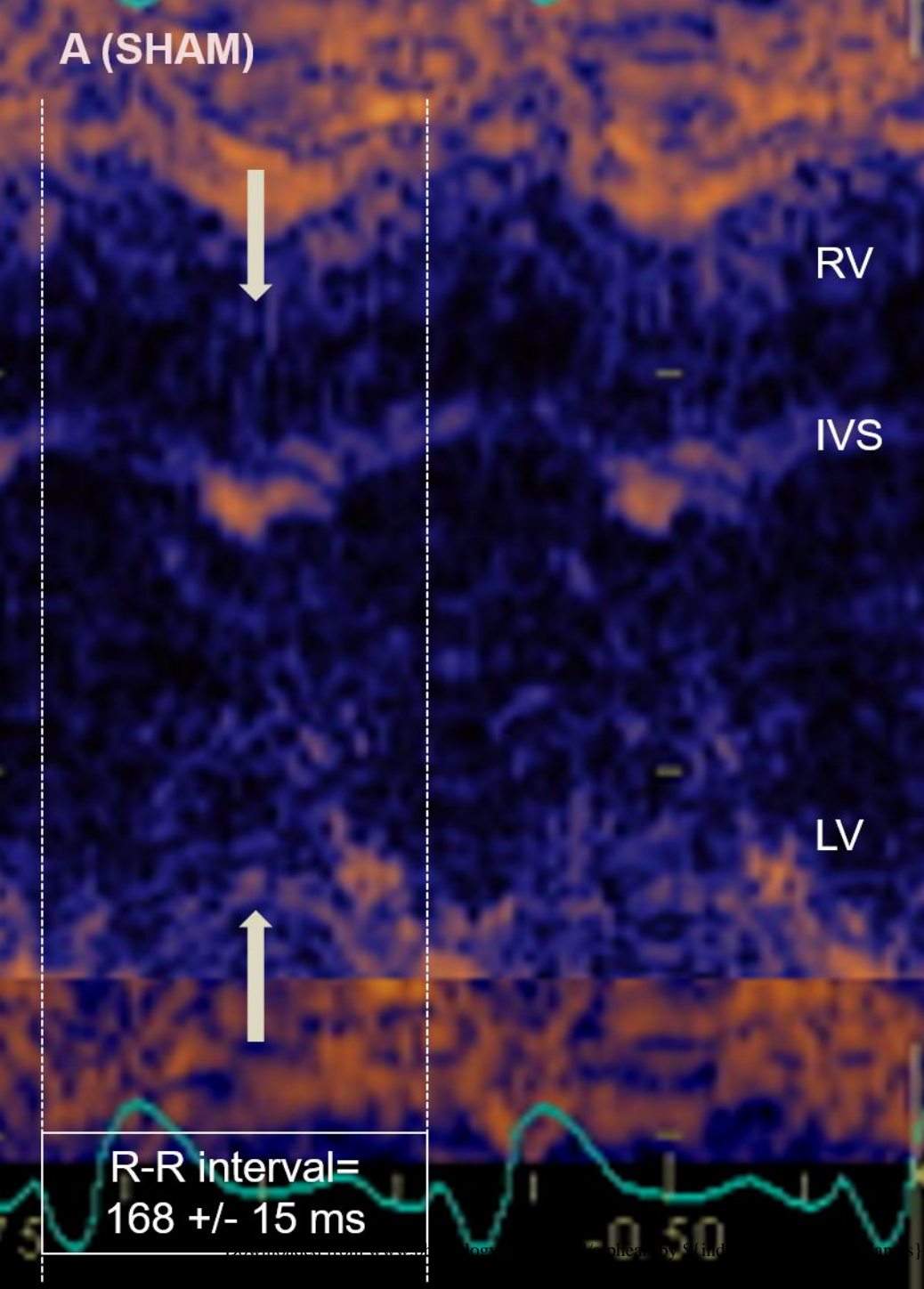




Figure 3 (A)



# B (MONOCROTALINE)

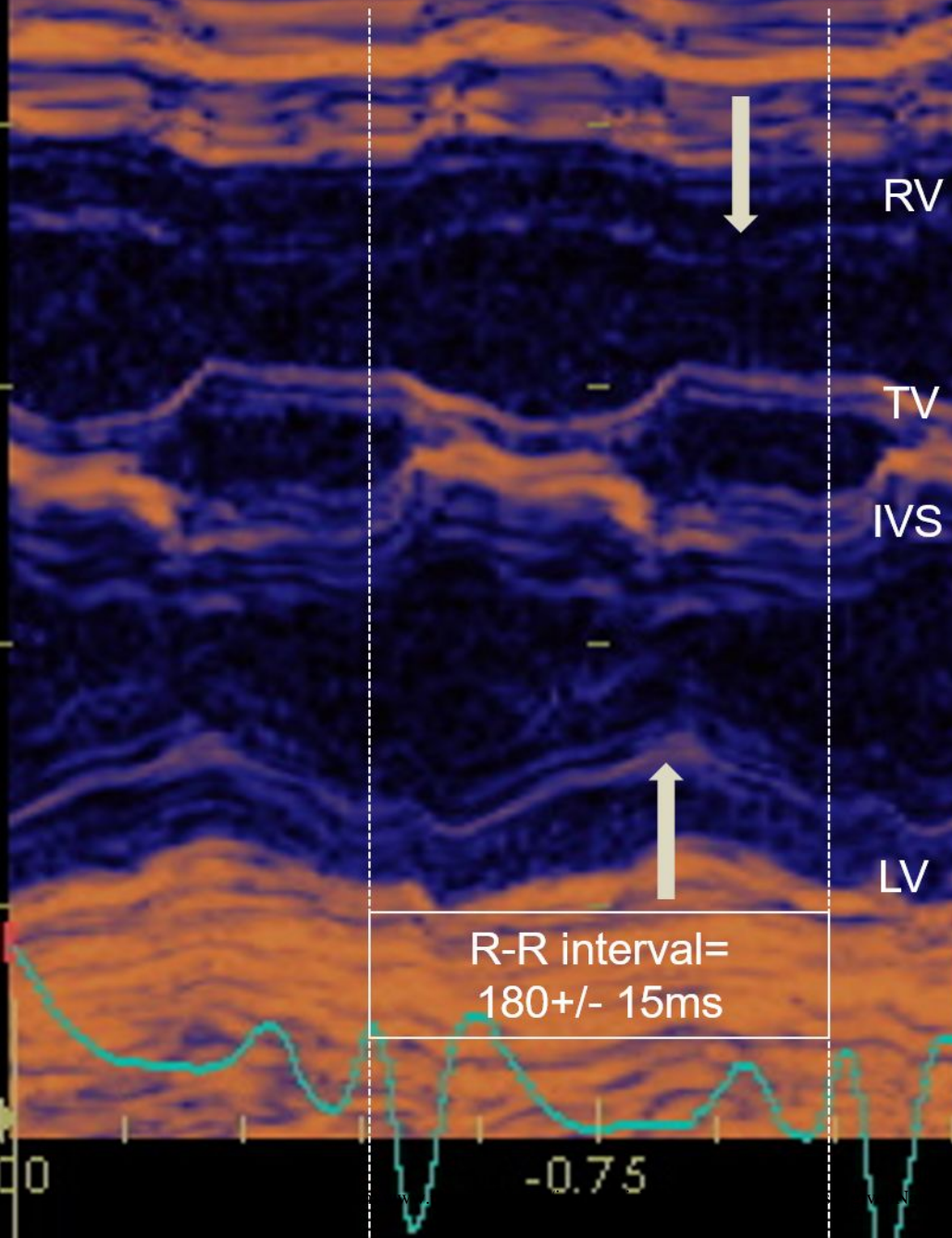
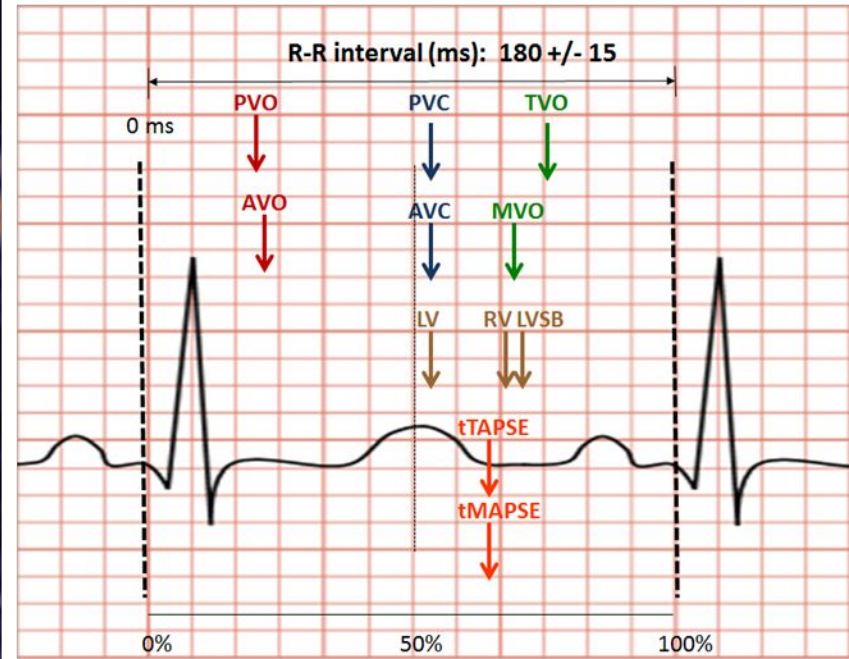


Figure 3 (B)





# C (CARVEDILOL)

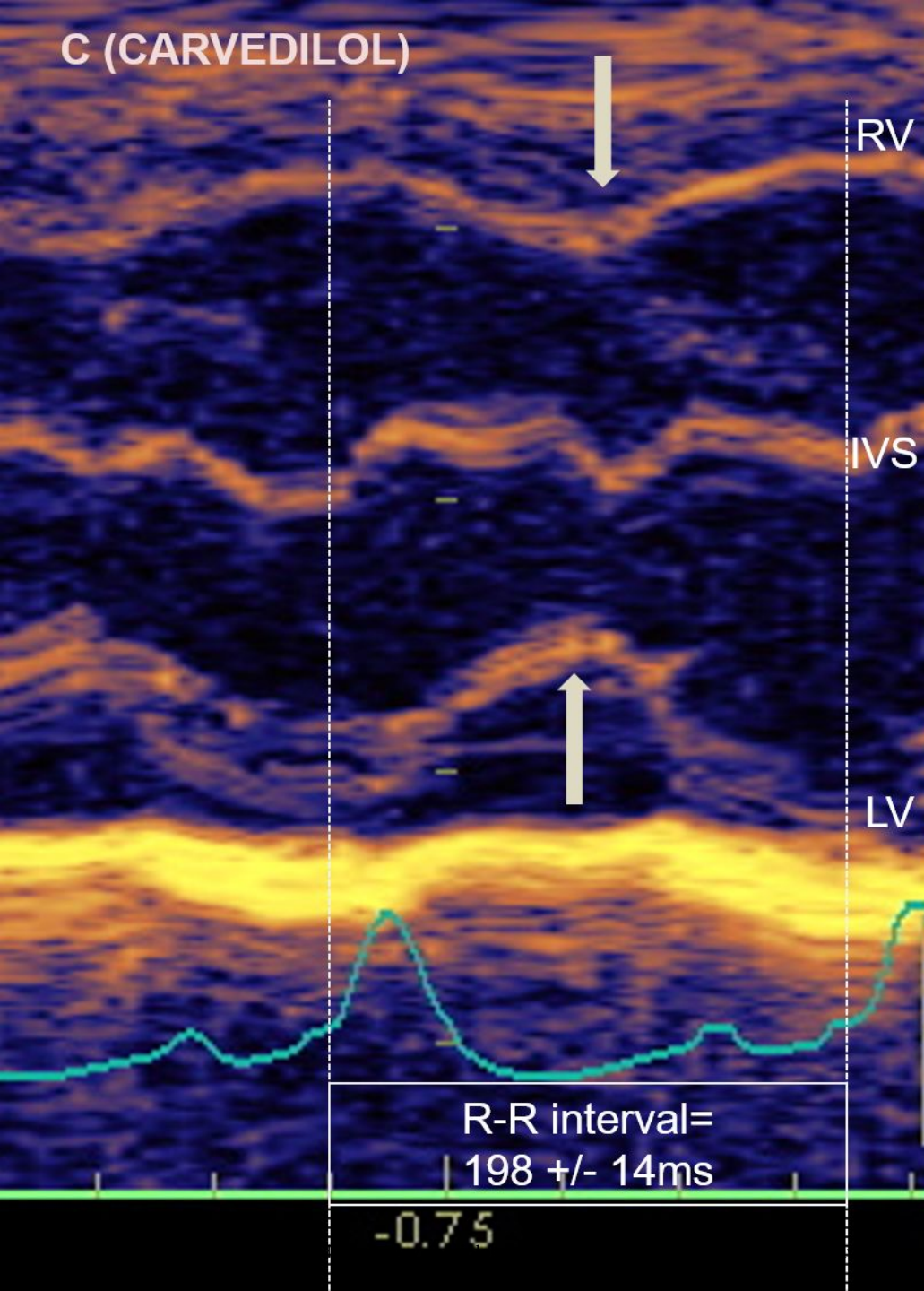
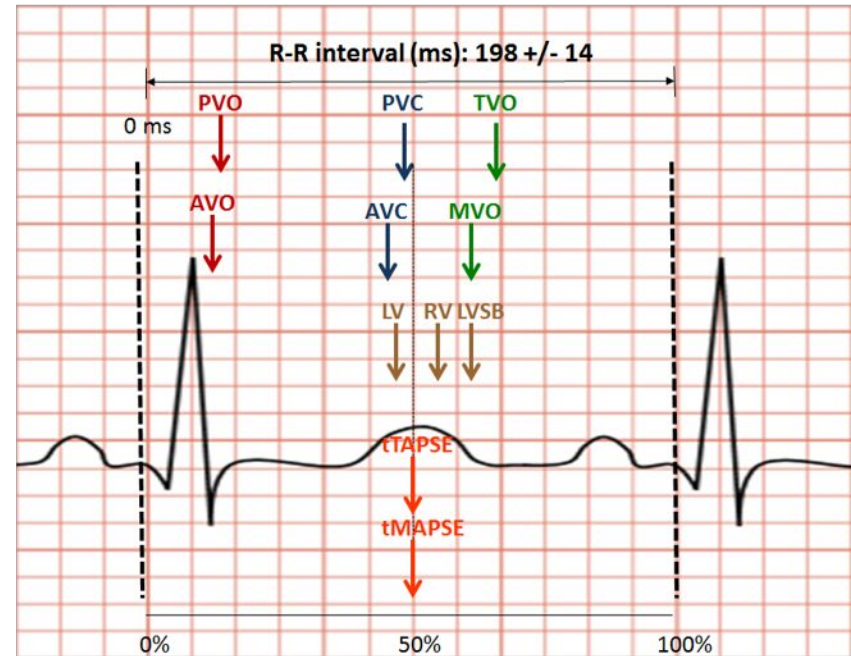


Figure 3 (C)



# D (IVABRADINE)

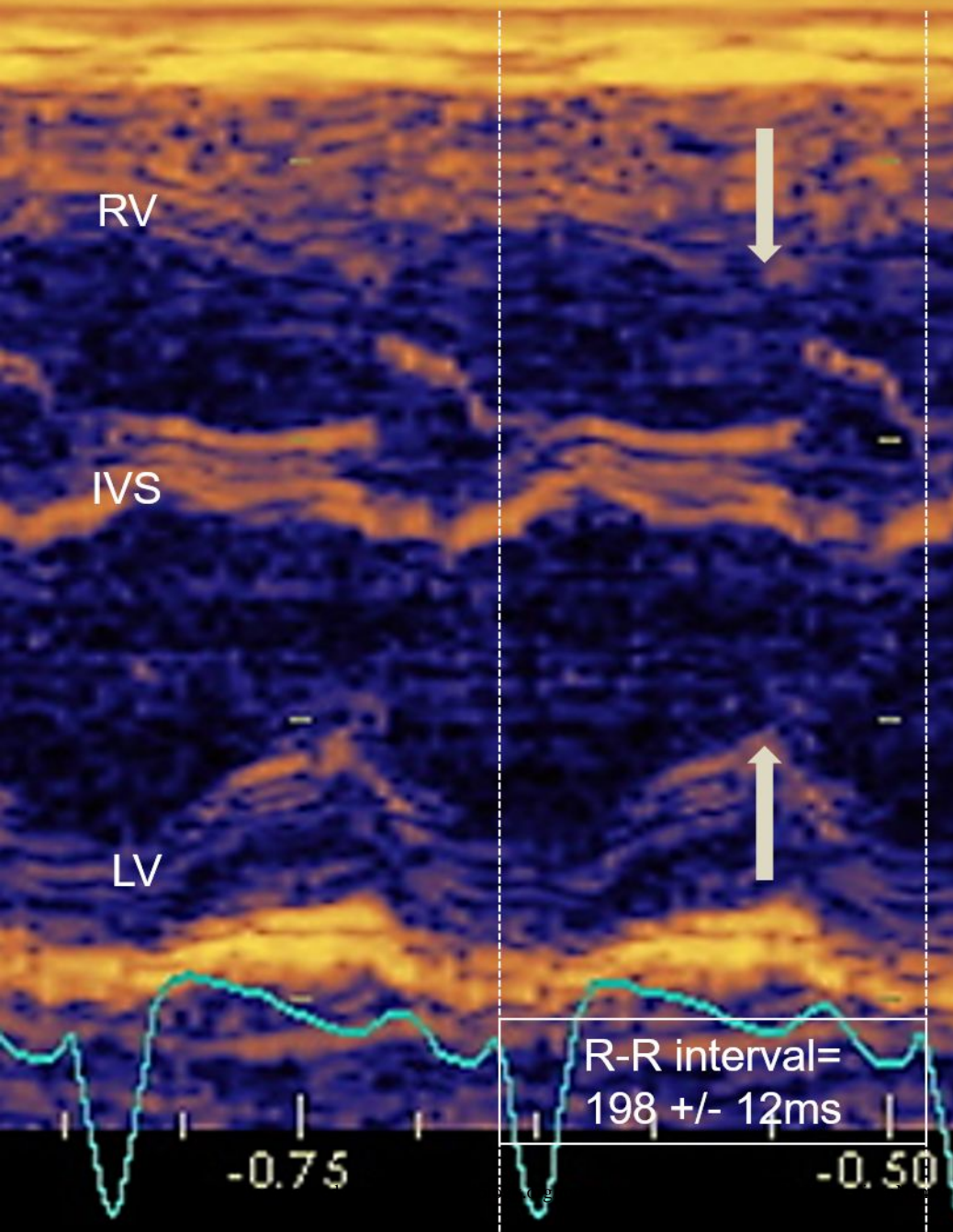
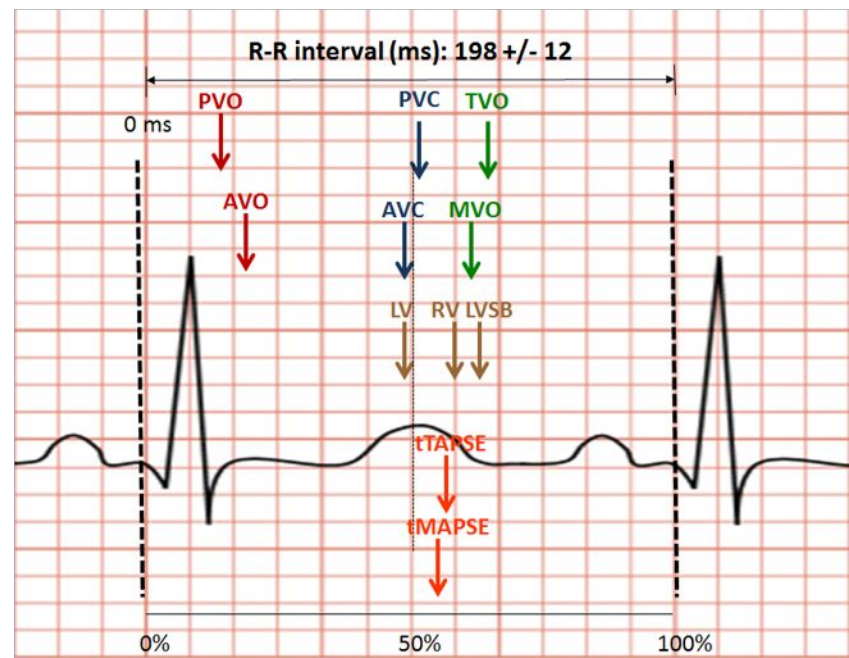


Figure 3 (D)





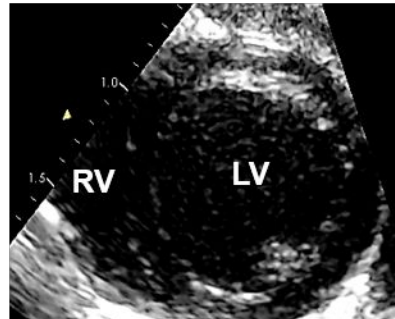
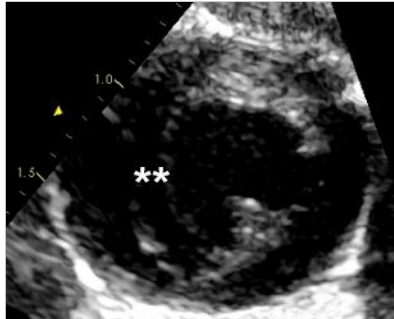
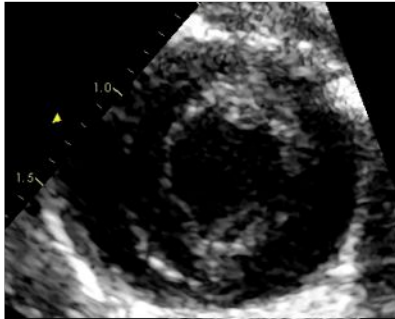
End-systole

Early-diastole

End-diastole

Figure 4

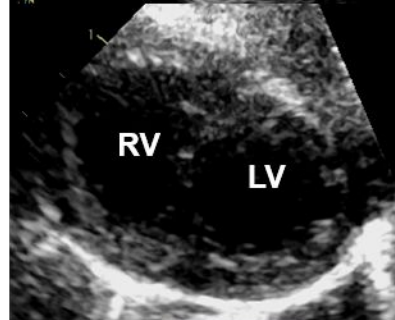
A)



B)



C)



D)

